



This is a repository copy of *Choosing a similarity index to quantify gait data variability*.

White Rose Research Online URL for this paper:

<https://eprints.whiterose.ac.uk/102991/>

Version: Accepted Version

Proceedings Paper:

Di Marco, R. orcid.org/0000-0002-3644-352X, Pacilli, A., Scalona, E. et al. (3 more authors) (2016) Choosing a similarity index to quantify gait data variability. In: Gait & Posture. XVII Congress of the Italian Society of Movement Analysis in Clinics SIAMOC, 05-08 Oct 2016, Milano, Italy. Elsevier .

<https://doi.org/10.1016/j.gaitpost.2016.07.032>

Reuse

This article is distributed under the terms of the Creative Commons Attribution-NonCommercial-NoDerivs (CC BY-NC-ND) licence. This licence only allows you to download this work and share it with others as long as you credit the authors, but you can't change the article in any way or use it commercially. More information and the full terms of the licence here: <https://creativecommons.org/licenses/>

Takedown

If you consider content in White Rose Research Online to be in breach of UK law, please notify us by emailing eprints@whiterose.ac.uk including the URL of the record and the reason for the withdrawal request.



eprints@whiterose.ac.uk
<https://eprints.whiterose.ac.uk/>

CHOOSING A SIMILARITY INDEX TO QUANTIFY GAIT DATA VARIABILITY

R. Di Marco^{1,2}, A. Pacilli¹, E. Scalona¹, S. Rossi³, C. Mazzà², P. Cappa¹

¹ Sapienza University of Rome, Rome, Italy, ² University of Sheffield, UK, ³ University of Tuscia, Viterbo, Italy

INTRODUCTION

Repeatability and reproducibility of joint kinematics can be assessed through Similarity Indices (SI) quantifying their pattern variability. These include: Coefficient of Multiple Correlation (CMC) [1]; Mean Absolute Variability (MAV) [2]; and Linear Fit Method (LFM) [3], which accounts for scaling (a_1), offset (a_0) and truthfulness of the linear model between the curves (R^2). Among gait cycles, the intra-subject variability for a given joint is due to physiological fluctuations of the range of motion (ROM) and time shift. SIs might be differently affected for each joint, due to their different ROMs, and by marker positioning, leading to offsets among gait curves. This paper aims to investigate the effects that each of these sources of curve variability has on the SIs, in order to provide indications on which is the most suitable for the assessment of gait similarity.

METHODS

Four groups of simulations were conducted to study the influence of each variability source on CMC, MAV and LFM coefficients, which were calculated on datasets composed by five synthetic curves [4]:

$$k(t) = O + \frac{1}{2} \left(ROM \pm \frac{A}{2} \right) \left[0.5 \sin \frac{2}{100} \left(\frac{t}{100} \right) + 0.5 \sin \frac{4}{100} \left(\frac{t}{100} \right) \right], \quad t \in [0, 100]$$

One variability source per time varied within each group of simulations, and across different datasets, specifically: (i) ROM (values: 5, 10, 20, 40, 60°); (ii) ROM fluctuation ($\Delta A\%$; values: 5, 10, 15, 20, 25, 30%_{ROM}), i.e. the percentage difference between maximum and minimum ROMs, normalized on the ROM averaged among strides; (iii) offset (O, values: 10, 40, 70, 100, 130, 160, 190%_{ROM}); (iv) time shift (τ , values: 5, 10, 15, 20%_{GaitCycle}). A ROM equal to 5° was set for cases (ii)-(iv). The criteria adopted to choose the previously mentioned ranges of variation was based on the lowest and the highest variability values obtained from gait data of the lower limb of ten healthy subjects [5].

RESULTS

CMC was always >0.99 for different ROMs, and was the least sensitive to variations of ROM fluctuation (>0.99 for all levels, except for $\Delta A\%=30\%$ with CMC=0.99). CMC decreased from >0.99 to 0.44 when O increased from 10%_{ROM} to 190%_{ROM}, and decreased from 0.98 to 0.73 when τ increased from 5%_{GaitCycle} to 20%_{GaitCycle}.

MAV increased when each source of variability increased: from 0.1° to 1.2° for ROM in the range of 5-60°; from 0.1° to 0.6° for $\Delta A\%$ in the range of 5-30%_{ROM}; from 0.5° to 9.5° in the range of 10-190%_{ROM}; from 1.1° to 3.8° for τ in the range of 5-20%_{GaitCycle}.

LFM was insensitive to different ROMs ($a_1=1.00 \pm 0.02$, $a_0=0.00 \pm 0.00^\circ$, $R^2=1.00 \pm 0.00$ for all levels), whereas $\Delta A\%$, O and τ affected a_1 , a_0 , and R^2 , respectively: a_1 varied from 1.00 ± 0.02 to 1.00 ± 0.10 for $\Delta A\%$ ranging from 5 to 30%_{ROM}, with $a_0=(0.00 \pm 0.00)^\circ$, $R^2=1.00 \pm 0.00$; a_0 ranged between $(0.00 \pm 0.2)^\circ$ to $(0.00 \pm 3.8)^\circ$ for O varying from 10%_{ROM} to 190%_{ROM}, with $a_1=1.00 \pm 0.00$ and $R^2=1.00 \pm 0.00$; a_1 varied from 1.00 ± 0.02 to 1.00 ± 0.23 , and R^2 from 0.97 ± 0.02 to 0.64 ± 0.28 for τ varying from 5%_{GaitCycle} to 20%_{GaitCycle} with $a_0=(0.00 \pm 0.2)^\circ$.

DISCUSSION

MAV showed no specialised behaviour with respect to the source of variability so it was not able to detect the leading cause for the variability among curves. CMC was not sensitive to ROM and, among the chosen indices, was the least sensitive to $\Delta A\%$. CMC decreased, instead, when τ and O increased, requiring further analysis to separate these two effects. Whereas, a_1 , a_0 , and R^2 were not sensitive to ROM, and are affected by $\Delta A\%$, O and τ , respectively. Thus, the results suggest using the LFM to assess gait data similarity, as it performs a more complete analysis on the data.

REFERENCES

- [1] Kadaba MP, et al. *J Orthopaed Res* 1989;7:849-860.
- [2] Ferrari A, et al. *Med Biol Eng Comput* 2010;48:1-15.
- [3] Iosa M, et al. *BioMed Research International* 2014;2014:7pp.
- [4] Røslie J, et al. *J Biomech* 2012;45:2014-18.
- [5] Leardini A, et al. *Gait Posture* 2007;25:453-462